INTERNAL STATE MEASUREMENT FROM FACIAL STEREO THERMAL AND VISIBLE SENSORS THROUGH SVM CLASSIFICATION

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ABSTRACT

Our main aim is to propose a vision-based measurement as an alternative to physiological measurement for recognizing mental stress. The development of this emotion recognition system involved three stages: experimental setup for vision and physiological sensing, facial feature extraction in visual-thermal domain, mental stress stimulus experiment and data analysis and classification based on Support Vector Machine. In this research, 3 vision-based measurement and 2 physiological measurement were implemented in the system. Vision based measurement in facial vision domain consists of eyes blinking and in facial thermal domain consists 3 ROI’s temperature value and blood vessel volume at Supraorbital area. Two physiological measurement were done to measure the ground true value which is heart rate and salivary amylase level. We also propose a new calibration chessboard attach with fever plaster to locate calibration point in stereo view. A new method of integration of two different sensors for detecting facial feature in both thermal and visual is also presented by applying nostril mask, which allows one to find facial feature namely nose area in thermal and visual domain. Extraction of thermal-visual feature images was done by using SIFT feature detector and extractor to verify the method of using nostril mask. Based on the experiment conducted, 88.6\% of correct matching was detected. In the eyes blinking experiment, almost 98\% match was detected successfully for without glasses and 89\% with glasses. Graph cut algorithm was applied to remove unwanted ROI. The recognition rate of 3 ROI’s was about 90\%-96\%. We also presented new method of automatic detection of blood vessel volume at Supraorbital monitored by LWIR camera. The recognition rate of correctly detected pixel was about 93\%. An experiment to measure mental stress by using the proposed system based on Support Vector Machine classification had been proposed and conducted and showed promising results.

Keywords: thermal face image analysis, facial feature extraction, thermal-infrared geometric camera calibration, blood vessel extraction.

INTRODUCTION

Various methods for internal state measurement such as mental stress have been previously proposed which utilizes the changes of physiological quantities such as blood pressure, heart rate, salivary amylase and electromyography (EMG) (Scheirer et al. 2002). These quantities can be measured invasively by the use of expensive instruments. In this paper we introduce an integrated non-invasive measurement through purely imaging means. The proposed booth setup is equipped with Thermal IR and Visual Camera Sensors. A monitor and a speaker are also installed to provide mental and acoustic stimulus to monitor changes in facial sign and brain waves. These experiments will be done at a later stage.

Face recognition system based on visual images have reached significant level of maturity with some practical success. However, the performance of visual face recognition may degrade under poor illuminations conditions, for subjects of various skin color and the changes in facial expression. The use of infrared in face recognition allows the limitations of visible face recognition to be overcome. However, infrared suffers from other limitations like opacity to glasses.

Multi modal fusion comes with the promise of combining the best of each modalities and overcoming their limitations (Moulay Akhloufi et al. 2008). Facial feature in thermal is difficult to locate because of the poorer contrast between the features and the face in IR images. In this paper, one common feature that can be automatically located in both thermal-visible domains is the nostril area. This is due to the changes of temperature in nostril area in thermal domain and the higher contrast value in visual domain.

The combined relationship includes two parts: 1) The relative position between the thermal and visible camera that are calibrated using special calibration board (Mohd Norzali et al. 2012), 2) The relative position and head pose based on nostril mask in thermal and visible. We have also analyzed the use of SIFT descriptor as feature matching in thermal and visual domain to verify our method using nostril mask.

This paper presents a novel methodology for real time monitoring of internal emotion state particularly mental stress. The method does not require any contact as contact measurement tend to effect emotions and burden physiologically. Based on recent study (J. Levine et al. 2001), (I. Pavlidis, 2002) and (Dvijesh, 2012) conducted, we have found out that user stress is correlated with the increased blood flow in three facial areas of sympathetic importance which is periorbital, supraorbital and maxillary. This increased blood flow dissipates convective
heat which can be monitored through mid-wave infrared (MWIR, 3-5µm) camera (Figure-2 (b)) (Zhen Zu, 2008). Our approach is different which is trying to implement it on a long-wave infrared (LWIR, 8-14µm) camera.

**PROPOSED SYSTEM**

**Image registration and calibration**

The relative position between the IR and visible cameras is calibrated by using the special calibration board suggested previously by (Z. Zhang et al. 2000). With some small adjustment and preparation where cold fever plasters are attached to the back of the calibration points on a chessboard, the calibration points can be reliably located in thermal IR and visible domain.

One of the common strategies to simplify correspondence problem between IR and visible domain is to exploit epipolar geometry (Figure-2 (b)). The relative position between thermal-visible stereo cameras is calculated using the heated calibration board which is due to the emissivity difference between the black and white squares on the grid. The output of the calibration method includes the relative rotation and translation of the cameras as well as the internal parameters.

**Calibration of thermal IR and visible stereo camera**

The output of the calibration method includes the relative rotation $R$ and translation $T$ of the cameras with respect to the left hand view and the internal parameters of each camera, focal length $f_c$, principal point $c_e$, skew coefficients $\alpha_c$ and radial and tangential distortion $k_c$. Following stereo calibration, coordinates of a 3D point, $p_c = [x_c, y_c, z_c]$, as follows $P_c = T + R P$, where $R$ and $T$ are their respective relative rotation and translation with respect to the world coordinates. Here, for the surface reconstruction procedure, we make use of the image point projection of the scene normalized so as to follow the pinhole camera model 10, Let the normalized (pinhole) image projection, $p_n = [x, y]$ be given by:

$$ p_n = \left[ \frac{x}{y}, \frac{y}{y} \right]. $$

After including the lens distortions, the new normalized point coordinates $p_d = [x_d, y_d]$ is obtained.
Where, and \( dx \) is the tangential distortion vector

\[
d_{x} = \left[ 2k_{c}(3)x + k_{c}(4)(x^2 + 2y^2) \right]
\]

With these ingredients, we can relate the normalized coordinate vector, \( p_{d} \), and the pixel image coordinates, \( x_{d} \) and \( y_{d} \) as follows

\[
\begin{bmatrix}
 x_{p} \\
 y_{p} \\
 1
\end{bmatrix} = K \begin{bmatrix}
 x_{d} \\
 y_{d} \\
 1
\end{bmatrix}
\]

(3)

Where \( K \) is known as the camera parameter matrix, which can be expressed making use of the calibration output variables as

\[
K = \begin{bmatrix}
 f(1) & a_{c} & c_{c}(1) \\
 0 & f(2) & c_{c}(2) \\
 0 & 0 & 1
\end{bmatrix}
\]

Facial feature extraction for thermal domain

Thermal face image analysis has many applications such as sensation evaluation and face recognition. Facial feature extraction in the IR image is an essential step in these applications. Certain facial areas such as periocular, nasal, cheeks and neck region produce different thermal patterns for different activities or emotions (Hartley R. and Zisserman A. 2000). Skin temperature of facial features, such as the nose and forehead, could be an effective indicator in objectively evaluating human sensations such as stress and fatigue (Dvijesh A. Merla et al. 2009) and (T.Shell et al. 2010). Most existing approaches manually locate the facial feature in IR image or the subject are required to wear marker[14], as it is hard to automatically locate facial features, even for the obvious features such as the corners of the eyes and mouth. This problem is caused by poorer contrast between the features and the face in IR images.

In our experiment, we have found out that by using the proposed face detection using Cascade structure with Haar-like in both Thermal and Visual can detect faces automatically. Measurement is done at three facial areas of sympathetic importance which is periorbital, supraorbital and maxillary (Figure-3). Based on the past researches (C.Puri et al. 2005) and (Jian-Gang Wang. et al. 2007) we have found out that 3 ROIs are the most affected during Mental Stress and focuses on the temperature in these areas.

In our experiment, at first, we detect the face region using Viola and Jones’s Boosting algorithm and a set of Cascade structure with Haar-like features. Then 3 ROIs are detected based on detected face ratio. The collaboration of ROI with temperature value was done based on the relationship as in [4].

This relationship is concluded through several experiments done to ensure the accuracy. The average brightness value located around these 3 main areas is then converted to the temperature value.

\[
\text{Temperature}=0.0819*\text{GrayLevel}+23.762
\]

(4)

Next, we assume that the centroid of the detected face area as nose area and nostril mask is used to recalculate the detected area and map into the facial thermal image (Figure-6).

We then analyze the detected thermal face with the 3 ROIs with sympathetic importance for person wearing spectacles and without it. We found out that there are unwanted ROI such as spectacles and hair which can be excluded so that temperature reading can be done precisely (Figure-4). To overcome this problem, unwanted ROI is removed by using Graph Cut method. We have concluded that the average differences before and after cropping is about 0.3-0.6 °C (Figure-5).
One of the most salient manifestation of sustained stress is that eyebrows frown frequently. The frowning is caused by contraction of the corrugator muscle. Activation of the corrugator muscle requires more blood, which is drawn from supraorbital vessels. Increased of the blood flow in the supraorbital vessels, directly increase the cutaneous temperature on the forehead. Our task is to detect elevated stress levels through quantification of increased vessel temperature in thermal imagery.

The proposed methodology for detecting blood vessel as in the Figure-9 (a). After the detection of supraorbital area in thermal IR, image morphology is applied on the diffused image to extract the blood vessels that are relatively low contrast compared with the surrounding tissue. We employ, top-hat segmentation method, which is the combination of the erosion and dilation operations. We are interested in the bright (hot) like structure which correspond to Blood Vessel. For this reason we employ White Top-Hat segmentation (WTH) as in equations (5).

$$I \circ S = (I \ominus S) \oplus S \quad (4), \quad WTH = I - (I \circ S) \quad (5)$$

where,

$I$: Original Image, $I \circ S$ : Opened Image, $I \bullet S$ : Closed Image, $S$: Structuring element, $\ominus$: Erosion, $\oplus$: Dilation.

In order to enhance the edge and reduce noise bilateral filter is then employed. Bilateral filter is a nonlinear, edge preserving and noise reducing smoothing filter. The intensity value at each pixel in an image is replaced by a weighted average of intensity values from nearby pixels.

$$f_{\text{filtered}}(x) = \sum_{x} f(x) f_{g}(y) g_{s}(||y-x||)$$

where $f_{\text{filtered}}$ is the filtered image; $f$ is the original input image to be filtered; $x$ is the coordinates of the current pixel to be filtered; $\Omega$ is the window centered in $x$; $f_{g}$ is the range kernel for smoothing differences in intensities. This function can be a Gaussian function; $g_{s}$ is the spatial kernel for smoothing differences in coordinates.

After applying bilateral filter, based on the RGB pixel value, the red range of pixel which is associated to blood vessel is then segmented (Figure-6 (a)).

The blood vessel at supraorbital recognition system (a) segmentation at supraorbital area, White top hat segmentation, bilateral filter and binary image. (b) Detected blood vessel during stress stimulus.

Facial feature extraction for visual domain

The same approach for locating face image in visual face is also done. At first we detect the face using Viola and Jones’ Boosting algorithm and a set of cascade structure with Haar-like features. Next, we assume that the centroid of the detected face area as nose area and nostril mask is used to recalculate the detected area and map into the facial image (Figure-7).

Figure-8, shows the propose blinking recognition system. After the detection of face based on cascade structure with Haar-like features, the eye part is located by calculating the edge of the eyes which is considered as the brightest part of the face. Next Integral Image is calculated to determine the exact location of eyes and iris. Then based on the pixel value of iris masking, blinking is determined. We then locate blink detection by the ratio of the white and black pixel detected mask. When the ratio is bigger than the threshold value, the eyes are considered open and when it is less, they are considered close.
Figure-8. (a) Blinking Recognition System Flow, (b) Face Recognition based on Cascade structure with Haar-like features, (c) Iris Masking (Eyes open), (d) Iris Masking (Eyes close state).

EXPERIMENTS AND RESULTS

To evaluate the alternative approaches and the effectiveness of the proposed calibration board, MRE (Multiple Regression Equations) [7] is used as the metric for comparison. In general, it is calculated using only frames included in the calibration process. We choose to calculate MRE using entire input that has not actually been selected for calibration. The units are in pixels.

$$\text{MRE} = \frac{\sum_{m=1}^{N} \sum_{n=1}^{M} ||p(m,n)-q(m,n)||}{MN} \quad (7)$$

M, is the total number of frames in the extended sequence, and N is the total number of calibration points per frame. p(m,n) is the pixel location of a point in the pattern, and q(m,n) is the projected location of that point using an estimate of the pose of the pattern in the particular frame.

The experiment is conducted in a normal office environment, with an ambient temperature of approximately 24°C. The calibration objects are placed at the minimum focal distances for which the pattern is fully visible, approximately 50cm from the lens. A workspace approximately 1m³ is required for the experiment.

The proposed calibration board is evaluated and compared with existing approaches for calibrating thermal and visual cameras. 100 calibration frames of each pattern are used to compare the performance.

Two types of chessboard are printed on an A4 sheet paper. One type which is the conventional chessboard and another is the fever plaster which is in the cool gel form is attached at the back of the chessboard as in Figure-2(a). A 500 W heat lamp is used for approximately 5s to heat the pattern as even as possible. Footage is then captured immediately for approximately 10s, at which point the image contrast had degenerated significantly. An identical software framework is used for both method. OpenCV function “find Chess board Corners ()” is used.

From Table-1, it is clear that calibration points on the proposed chessboard FCP can be more clearly located than those on the standard chessboard.

<table>
<thead>
<tr>
<th>Configuration</th>
<th>MRE</th>
</tr>
</thead>
<tbody>
<tr>
<td>Thermal (chessboard)</td>
<td>0.814±0.015px</td>
</tr>
<tr>
<td>Thermal (FCP)</td>
<td>0.614±0.011px</td>
</tr>
</tbody>
</table>

Table-2. Intrinsic parameters of the two cameras.

<table>
<thead>
<tr>
<th>Camera</th>
<th>Thermal Camera (right)</th>
<th>Visual camera(left)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Matrix</td>
<td>274.02  0  140.08</td>
<td>272.34  0  157.3</td>
</tr>
<tr>
<td>Optical coefficients</td>
<td>K1: -0.39235</td>
<td>K1: -0.42247</td>
</tr>
<tr>
<td></td>
<td>K2: 0.25438</td>
<td>K2: 1.1306</td>
</tr>
<tr>
<td></td>
<td>P1: 0.001792</td>
<td>P1: -0.001560</td>
</tr>
<tr>
<td></td>
<td>P2: 0.0051091</td>
<td>P2: 0.0064488</td>
</tr>
</tbody>
</table>

Table-3. Extrinsic parameters of the two cameras relating to its position.

In the experiment conducted, Scale Invariant Feature Transform (SIFT) is employed to extract facial features in both thermal and visual and to verify our algorithm. SIFT features are features extracted from images to help in reliable matching between different views of the same object. The extracted features are invariant to scale and orientation, and are highly distinctive of the image. They are extracted in four steps. The first step computes the locations of potential interest points in the image by detecting the maxima and minima of a set of Difference of Gaussian (DoG) filters applied at different scales all over the image. Then, these locations are refined by discarding points of low contrast. An orientation is then assigned to each key point based on local image features.

Finally, a local feature descriptor is computed at each key point. This descriptor is based on the local image gradient, transformed according to the orientation of the key point to provide orientation invariance. Every feature
is a vector of dimension 128 distinctively identifying the neighborhood around the key point.

Figure-9. (a) Nostril mask in thermal, (b) Facial sift feature in visual (c) Sift feature matching.

At first, the nostril area in thermal IR is detected using our pair calibrated Thermal –Visible camera. Then, the face part in visible domain is detected and SIFT feature point is calculated in both domain (Figure-9). The feature matching is done and recorded as in Table-4.

Table-4. Feature matching between nostril mask (Thermal)- Visible camera.

<table>
<thead>
<tr>
<th>Frame</th>
<th>Feature Point 1 (T)</th>
<th>Feature Point 2 (V)</th>
<th>Processing Time [ms]</th>
<th>Correct Matching</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>2</td>
<td>157</td>
<td>170.759</td>
<td>100</td>
</tr>
<tr>
<td>2</td>
<td>2</td>
<td>93</td>
<td>168.443</td>
<td>100</td>
</tr>
<tr>
<td>3</td>
<td>11</td>
<td>160</td>
<td>171.860</td>
<td>36</td>
</tr>
<tr>
<td>4</td>
<td>2</td>
<td>81</td>
<td>162.892</td>
<td>100</td>
</tr>
<tr>
<td>5</td>
<td>2</td>
<td>168</td>
<td>170.521</td>
<td>50</td>
</tr>
<tr>
<td>6</td>
<td>1</td>
<td>168</td>
<td>154.102</td>
<td>100</td>
</tr>
<tr>
<td>7</td>
<td>1</td>
<td>114</td>
<td>160.873</td>
<td>100</td>
</tr>
<tr>
<td>8</td>
<td>1</td>
<td>112</td>
<td>153.269</td>
<td>100</td>
</tr>
<tr>
<td>9</td>
<td>1</td>
<td>146</td>
<td>170.35</td>
<td>100</td>
</tr>
<tr>
<td>10</td>
<td>1</td>
<td>157</td>
<td>170.972</td>
<td>100</td>
</tr>
</tbody>
</table>

To evaluate our methodology, the experiment is conducted towards 5 subjects, tested for two times of stress stimulus experiment. The reason for conducting two times test to the subjects is to ensure that the subjects are free from any kind of stress. The subjects are also given 1 minute rest to make them calm and neutral. We utilise the stress test which is very well established method for inducing stress. Mental stress experiment, Colour word stroop test is designed by Dr Soren Brage of MRC Epidemiology unit, Cambridge University, which consists of 2 minutes test (120 Slides), 30 seconds rest and 2 minutes test (120 Slides). About 20 people age from 18-30 both male and female participated in this study. The subject were asked to sit comfortably in the screening station and have him/her rest before and after the stimulus test. Verbal response were recorded in thermal and visual domain throughout the experiment. Our screening environment consists of light and sound proof screening station, NEC TH7800 thermal camera and USB CMOS imaging source DFK 22AUC03, stimulus screening monitor, temperature and humidity sensor for monitoring screening station PICO RH-02, pulse oximeter SAT-2200 to monitor pulse rate responder seat and operator machine.

Figure-10. a(1)-e(1) Temperature of 5 subjects for the first time stimulus experiment conducted. a(2)-e(2) Temperature of 5 subjects for the second time stimulus experiment conducted. (average booth temperature :27.75 C, average booth humidity:43%)(A: 1 minutes before stimulus , B-E: Subsequent 1 minutes during stimulus, B:1 minutes after stimulus).

In Figure-10. a(1)-e(1), 3 ROIs temperature differences are monitored for the first time. Subject is introduced with the stimulus test. Changes are detected mainly in the supraorbital areas. Out of 5 person, 2 person show visible blood vessel. Throughout the experiment, changes of temperature can be seen in the maxillary area.
In Figure-11 (a)-(d), 3 ROIs temperature differences monitored for the 2nd time when subject is introduced with the stimulus test. Changes are also detected in the supraorbital areas where 2 out of 5 persons show visible blood vessel. Temperature changes can be seen in the maxillary area.

Second experiment to monitor 3 ROI’s temperature before, during and after stimulus experiment was conducted and shows better result as Figure-11. In overall, during pre-stimulus which was 1-2 min, temperature in the 3 ROI’s was stable in the value. During stimulus, which was 2-4 min and 4-6 min, the temperature fluctuated and slight increase tendency can be seen. During rest time which was 4-5 min, there was a slight decrease of temperature at 3ROI’s and it increased gradually after the period. During post stimulus which was 6-7 min, the temperature in 3 ROI’s were stable and slight temperature decrease tendency can be seen. In most cases, especially in Figure-11(d) supraorbital area was most hottest part followed by periorbital and maxillary.

One of the most salient manifestation of sustained stress is that eyebrows frown more frequently (Zhen Zu, 2008). The frowning is caused by contraction of the corrugator muscles. Activation of the corrugator muscles requires more blood, which is drawn from supraorbital vessel. Increase blood flow in supraorbital vessels, directly increases the cutaneous temperature on the forehead. Therefore, mental stress is highly correlated with the activation of the corrugator muscle on the forehead.

Figure-12 shows the result when using (LOOCV) leave-one-out cross validation which increase the reliability of the result. SVM analysis show promising correlation between emotional stress and the physiological measurement. When using 7 features the recognition rate was 88.9% and decrease to 87.77% when using 6 features were salivary amilase is removed. It proof that the importance of salivary amilase measurement as well as pulse rate measurement.

**Figure-12.** Confusion matrix for stress detection using SVM (shaded cells are the number of correctly recognized affective state).

**DISCUSSION AND CONCLUSIONS**

We have developed an Automatic Thermal Face, Supraorbital, Periorbital, Maxillary and Nostril Detection to be used for estimation of internal state. Several faces samples are taken in real time in our experimental setup to measure the effectiveness of our method. Almost 98% of correct measurement of ROI and temperature is detected. Feature matching experiment is also done to measure the
effectiveness of our method of using nostril mask and shows positive results.

In the experiment which is monitoring the 3 ROIs temperatures before, during and after the stress stimulus, experiment was conducted 2 times. Thermal facial image also was monitored for possible blood vessel which is visible through the stress experiment. We have found out that user stress is correlated with the increased blood flow in three facial areas of sympathetic importance which is periorbital, supraorbital and maxillary.

Mental stress is highly correlated with the activation of the corrugator muscle on the forehead. However segmenting the thermal imprints of the supraorbital vessels is challenging because they are fuzzy due to thermal diffusion and exhibit significant inter-individual and intra-individual variation. On the average the diameter of the blood vessels is 10-15µm, which is too small for accurate detection and 0.1°C warmer that the adjacent skin.

### Table-5. Evaluation of Proposed Approach.

<table>
<thead>
<tr>
<th></th>
<th>Chestboard</th>
<th>FCP Chessboard</th>
</tr>
</thead>
<tbody>
<tr>
<td>Manufacturing</td>
<td>Printable from a standard printer</td>
<td>Printable from a standard printer with cheap fever cold plaster</td>
</tr>
<tr>
<td>Heating</td>
<td>A powerful (500W+) flood lamp and an external power supply are required. Difficult to get even coverage.</td>
<td>A powerful (500W+) flood lamp and an external power supply are required. Easy to get even coverage.</td>
</tr>
<tr>
<td>Footage</td>
<td>The pattern is only effective for a few seconds after heating.</td>
<td>The pattern can be used easily and effectively for about 15-30 minutes.</td>
</tr>
<tr>
<td>Searching</td>
<td>Generally requires preprocessing (inversion/thresholding). Many conventional algorithms will struggle to find the pattern automatically.</td>
<td>The algorithms are very common. No preprocessing required.</td>
</tr>
<tr>
<td>Accuracy</td>
<td>Less (see experiment)</td>
<td>Higher (see experiment)</td>
</tr>
</tbody>
</table>

The comparison between traditional heated chessboard and FCP is shown in table 5. The cost involved in manufacturing FCP Chessboard is considered cheap in comparing to other calibration board made from polished copper plate coated with high emissivity paint or calibration rig. Even though heating is required in both method, it is difficult to get an even coverage comparing to our method. The pattern also can last longer about 20 minutes.

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### REFERENCES


